



**SYNTHESIS AND CHARACTERIZATION OF FISH GELATIN
NANOPARTICLE AND ITS ROLE AS THE DRUG DELIVERY VEHICLE FOR
TUBERCULOSIS**

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ABSTRACT

Nanoparticle based systems have significant prospective for diagnosis, treatment and prevention of tuberculosis (TB) Gelatin nanoparticle derived from marine sources (fish skin, bone and fins) has been looked upon as a possible alternative to bovine and porcine. Fish gelatin nanoparticle synthesis by two step desolvation method, it was stable nanoparticles and confirm through Scanning electron microscopy (SEM). These nanoparticle were used as carrier for rifampicin. Our aim to develop a Nano particulate carrier of rifampicin for controlled delivery as well as reduced toxicity. In this study, rifampicin loaded fish gelatin nanoparticle was fabricated by an absorption/adsorption method. The effect of several variables on the Nanoparticle's characteristics was calculated.

Key words: Drug delivery, Nanoparticle, Gelatin, Tuberculosis, SEM, Fish gelatin

1.1 INTRODUCTION

Nanotechnology can be defined as the science and engineering involved in the design, Synthesis, characterization, application materials and devices whose smallest functional organization in at least one dimension is on the nanometer scale (One billionth a meter greatest values nanotech will be in the development of new and effective

medical treatments. Research into the delivery and targeting if therapeutic and diagnostic agents with nanoparticles is at the forefront, if Nano medicine for several reasons. First traditional oral or inject able drugs are not necessarily the most efficient formulations for a given product. This is particularly true for new biologics such as proteins and nucleic acids that require novel delivery

technologies to optimize efficacy, minimize side effects and lead to better patient compliance. These reformulation drugs have the potential advantages of drug side effects, increasing patient compliance, and reducing health care costs. (Dwaine, *et al.*, 2006). Several reports are available regarding the use of carrier systems like liposomes, dendrimers, micro spheres, and solid, lipid nano particles for delivery of bio actives.

Nano materials derived from proteins, especially protein nanoparticles are biodegradable, non- antigenic, metabolizable and can also be easily amenable for surface modification and covalent attachment of drugs and ligands. Because of the defined primary structure of proteins the protein based nanoparticles may suggest various possibilities for surface alteration and covalent drug attachment. Now a day's active research is focused on the preparation of nanoparticles using proteins of nanoparticles using proteins like albumin gelatin, gliadin and legumin (Mohsen,*et al.*, 2008) Gelatin is one of the protein materials that can be used for the production of nano particles. It's derived by hydrolytic degradation of collagen, the principle component of animal connective tissue. Raw materials from fish and poultry have received considerable attention in recent years. As for as fish gelatin is concerned the huge number of species having very different intrinsic characteristics. This range from natural resources like fish to polymers, the fish gelatin has been obtained from fish skin products and formulated as natural

hollow capsules of fish oil, spirulina and cellulose. (HabibaiBenta,*et al.*, 2011)

Gelatin from marine sources (warm and coldwater fish skins, bones, and fins) is a possible alternative to bovine gelatin. One major advantage of gelatin sources is that they are not associated with the risk of outbreaks of bovine spongiform Encephalopathy. Furthermore, Fish Skin, which is a major byproduct of the Fish processing industry, causing waste and pollution, could provide a valuable source of gelatin. Gelatin has been extracted from skins and bones of various cold water (e.g., cod, haddock, Alaska Pollock, and salmon) and warm water (e.g. Tuna, Catfish, Tilapia, Nile perch and Shark) fish.

NANOTECHNOLOGY IN TREATMENT OF TUBERCULOSIS

Treatments with improved sustained release profiles and bioavailability can increase compliance through reduced drug requirements and there in minimize chemotherapy of TB is complex due to the requirement of multidrug regimens that need to be administered over long periods. The poor patient compliance is the single most common reason for chemotherapy failure in TB. Carrier or delivery systems such as liposome's and micro spheres have been developed for the sustained delivery of antiTB drugs and have found better chemotherapeutic efficacy. The advantages of nanoparticles as drug carriers, high stability, high carrier capacity, feasibility of incorporation of both hydrophilic and hydrophobic substances; and feasibility of variable routes of administration, including oral

administration and inhalation. Jithendra Prasad mathuria, 2009 summarizes on nanoparticulate formulations of the antiTB drugs.

2. MATERIALS AND METHODS

2.1 MATERIALS

Cat fish (*Ictalurus punctatus*) 400-500g bought from a local market, filleted, washed and the skins were collected. The skins were weighed, packed in polyethylene bags and freeze stored at -20°C if not used immediately. All reagents used in the studies were of analytical grade. Rifampicin purchased from drug stores. *Mycobacterium tuberculosis* obtained from Asaripallam Government Medical College.

2.2 EXTRACTION OF FISH GELATIN

The procedure was essentially based on a mild acid pretreatment for collagen swelling, followed by extraction in water at moderate Temperature (45°C). The entire process takes about 24hrs. Because of the acid liability of the cross links found in fish skins collagen. Skins were washed under running tap water to remove superfluous materials. The wash skins were drip dried and soaked in the saturated lime solution [$\text{Ca}(\text{OH})_2$], at 20°C for 14 days for each kilogram of wet skins. $\text{Ca}(\text{OH})_2$ solution was used at the soaking medium. After soaking, the skins were then removed and washed with abundant tap water (1:10) to remove excessive $\text{Ca}(\text{OH})_2$ while maintaining the skins at pH 10. This was followed by the soaking in distilled

water at 48°C overnight to solubilize the gelatin. The solution was then filtered through whatman No 541 filter papers before passing through a strong acid cationic exchange resin, which reduced the pH of gelatin to approximately 5. The filtrates were then freezing, dried and analyzed for physio chemical properties (Jamilah, *etal.*, 2011).

The better recovery of gelatin is based on the wet and dry conditions of the skin and the use of $\text{Ca}(\text{OH})_2$ prior to gelatin extraction. The yield of gelatin was calculated using the following expression

$$\% \text{ of yield (wet weight basis)} = \frac{\text{Dry weight of gelatin}}{\text{Wet weight of skin}} \times 100$$

Wet weight of skin

2.3. FABRICATION METHODS OF GELATIN NANO PARTICLES

Two fundamental methods of cross linking have been described for gelatin Physical and chemical. Physical methods include UV irradiation and dehydrothermal treatment, although these are inefficient and make it difficult to control the cross linking density of the gelatin matrix. Chemical cross linking agents have been categorized into two types as non zero length and zero length. Non zero length cross linkers are functional or poly functional and operate by bridging free carboxylic acid residues or amine groups between adjacent protein molecules, e.g., glutaraldehyde (Simon, *et, al.*, 2005).

GNP was prepared by a two-step desolvation method with slight modifications. Briefly 10g gelatin was

dissolved in distilled water (100ml) under constant heating at $40\pm 1^{\circ}\text{C}$. Acetone (50ml) was added to the gelatin solution as a desolvation agent to precipitate the high molecular weight (HMW) gelatin. The supernatant was discarded, and the HMW gelatin was redissolved by adding distilled water (10ml) with stirring at 600rpm under constant heating. The pH of the gelatin solution at the second desolvation step was adjusted (between 2 and 12) drop wise addition of acetone (30ml) to form GNPs. At the end of the process, glutaraldehyde solution (25% V/V aqueous solution) was added 2 μl . It acts as a cross linking agent, and the solution was stirred for 12 hours at 600rpm. Effect of parameters like pH, temperature, amount of glutaraldehyde was studied (Manoj, *et al.*, 2008).

2.4. PHYSIO CHEMICAL TESTS

After gelatin production by above mentioned methods, quality factors were determined according to national and international standards.

2.4.1. PROTEIN CONFORMATION TEST

Biuret test for gelatin aqueous sample is treated with an equal volume of 1% strong base (sodium or potassium hydroxide most often) followed by a few drops of aqueous copper (II) sulfate. If the solution turns purple color.

2.4.2. COLOR DETERMINATION

Color of gelatin samples were measured by putting them on white background and compared with each other. Gelatin color must be pale yellow to amber (Hamid Tavakolipour, 2011).

2.5. CHARACTERIZATION THE NANOPARTICLES (FGNP)

2.5.1. SHAPE AND SIZE.

The morphology of FGPs was determined by Scanning Electron Microscopy (ZEISS from Carl Zeiss, India). A Scanning Electron Microscope (SEM) is a type of electron microscope that images a sample by scanning it with a beam of electrons in a raster scan pattern. The electrons interact with the atoms that make up the sample producing signals that contain information about the sample's surface topography, composition, and other properties such as electrical conductivity. The powdered sample was coated with gold and the accelerating voltage of 95KV.

2.6- DRUG LOADING

Drug loading can be done by two methods namely an Incorporation method and an Adsorption/absorption technique. Ideally, a successful Nano particulate system has a high drug loading capacity.

Adsorption /absorption technique followed to drug loading, absorbing the drug after formation of nanoparticles by incubating the carrier with a concentrated drug solution. Drug loading of nanoparticles was determined by the method proposed by the amount of RIF loaded was determined by incubating the nanoparticle suspension (1.0ml) in 5.0ml phosphate buffer saline (pbs.pH 7.4) for 2hrs at 800rpm at $25\pm 1^{\circ}\text{C}$.

The amount of unloaded and loaded drug was determined UVspectrophotometrically in the

supernatant obtained after separation of nanoparticles by centrifugation. The instrument used here was P.C based UV 5704SS Spectrometer. It consists of a spectrophotometer unit and a computer unit. The amount of radiant energy absorbed by a sample at a certain wavelength depends on how much of that substance, which absorbs that wavelength of radiation, is present in the sample. In other words, the absorption of radiant energy is proportional to the absorbing materials. Transmittance (T) is defined as the ratio of intensity of transmitted light and intensity of the light that is falling upon the sample when light falls upon a homogenous medium a portion is transmitted. It is the transmitted light that is actually detected by the instrument.

2.6.1 DRUG RELEASE STUDIES

Drug release from known amounts of RIF loaded FG nanoparticles was evaluated using the equilibrium dialysis technique at $37 \pm 1^\circ\text{C}$ and quantification was carried out by spectrophotometric method. Briefly, 2ml of nanoparticle dispersion was put in the dialysis bag (MWCO 3500 Da, Himedia, India) and were dialyzed against 50ml of PBS (pH 7.4) with 200mg /ml ascorbic acid, which was added as an antioxidant to prevent oxidative degradation of RIF at a rotation speed of 50 rpm. At predetermined time intervals, 0.5ml samples were withdrawn through sampling portion filtered through 0.45 micro meter membrane filter and the drug content was determined spectrophotometrically.

2.7 ANTIBACTERIAL ACTIVITY ASSAY WITH DISC DIFFUSION METHOD

Mycobacterium tuberculosis was added onto the L.J. medium and spread uniformly using a spreading tool. After that, the gelatin nanoparticles with drug loaded and drug unloaded were placed in the form of disks on the medium. It was kept under observation for seven days. It was evident that the antibacterial efficacy of the drug loaded gelatin nanoparticles was found to be higher than that of the pure gelatin nanoparticles, from the zone of inhibition. Wells with 8 mm diameters were prepared by punching a sterile cork borer onto the agar plates.

3. RESULTS AND DISCUSSIONS

3.1. Preparation and Characterization of Fish Gelatin

Fish gelatin manufacturing process consists of three main stages namely Pretreatment of the raw material, extraction of gelatin, purification and drying. Fish gelatin extracted using an acidic treatment is most suitable for the less covalently cross-linked collagen found in the skin of the fish. The parameters affecting the process include temperature, time and pH. Preparing fish gelatin typically involves a mild chemical pretreatment of the raw material and requires mild temperature conditions during the extraction process.

Raw materials stained were washed under running tap water to remove superfluous material and the steps mentioned in the extraction procedure were performed. On average, the extraction yield of fish gelatin was found to lie approximately between 6%

and 19% (expressed as grams of dry gelatin per 100g clean skin). The extracted fish gelatin was filtered and then freeze dried. The yield of gelatin was found to be 20% for 500gms of fish skin taken.

3.1.1 Protein Confirmation

An aqueous sample is treated with an equal volume of 1% strong base (sodium or potassium hydroxide most often) followed by a few drops of aqueous copper (II) sulfate. If the solution turns purple, protein is present. The color of the dried fish gelatin and fish gelatin solution was evaluated by judging the intensity of the intensity of fishy odor. Color of the gelatin sample was measured by putting them on a white background and comparing with each other. Fish gelatin color was pale yellow to amber.

3.2 PREPARATION OF FISH GELATIN NANOPARTICLES

Fish gelatin nanoparticles prepared using modified double desolvation method with acetone as the desolving agent and glutaraldehyde as the

crosslinking agent was found to be highly stable in water. The sediment obtained after first desolvation step mainly possessed the high molecular weight fish gelatin, while the supernatant which was removed, was containing portions of gelatin. The purpose of removing gelatin of low molecular weight was to avoid wider distribution of gelatin, which may not only cause formation of irreversible aggregates after crosslinking, but also form unstable particles. Acetone slowly added to protein solution acts as the desolvating agent. With the addition of acetone, a change occurs in the third structure of protein. When a certain level of desolvation was reached, protein clump was formed. In the next stage, nanoparticles were obtained when cross linked with glutaraldehyde. In order to obtain dispersed nanoparticles, we must stop the system before particles start to accumulate. System turbidity will be increased owing to the desolvation factor. Particles started to accumulate when the turbidity of the system were increased.



Fig 1: Preparation of fish gelatin nano particle

3.3. PARTICLE MORPHOLOGY:

The average particle size of FGNP_s was found to be 300 nm. Scanning electron microscopy was used to determine the shape and surface morphology of the nanoparticles

produced. Particles were coated with gold under vacuum before SEM analysis. It was found that the particle size and size distribution are the most important characteristics of nanoparticle system.

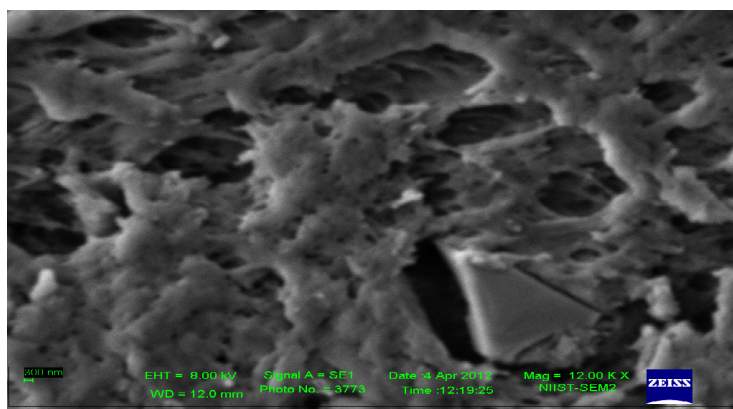


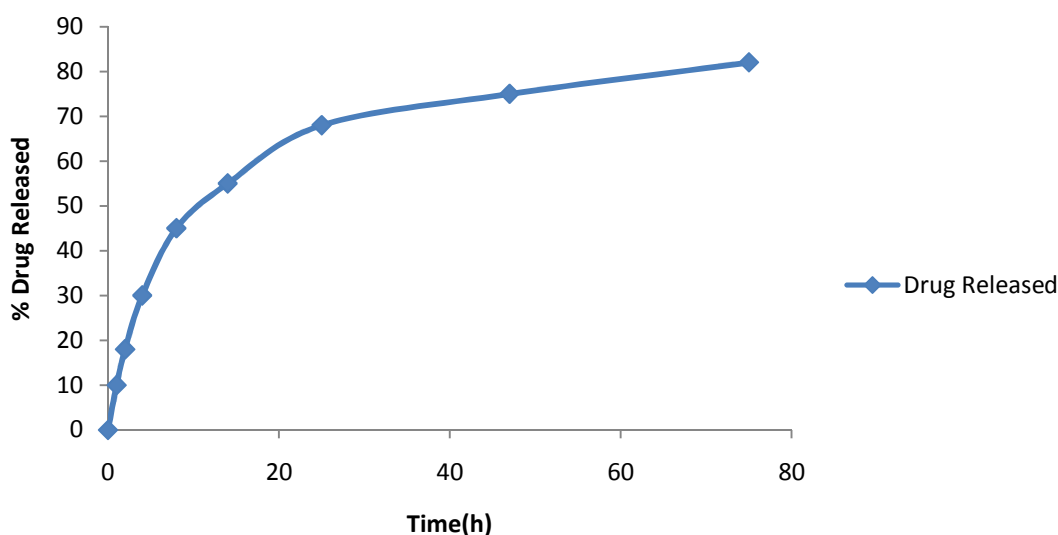
Fig 2: SEM micrograph for fish gelatin nanoparticle.

3.4. DRUG LOADING: Drug loading depends much on the solubility of the solid state drug in a matrix material and the molecular weight. UV-Vis spectra of pure RIF as well as RIF loaded FGNP_s were obtained using UV-Vis spectrophotometer. Transmittance (T) is defined as the ratio of intensity of transmitted light and intensity of the light that is falling upon the sample. In drug loaded nanoparticles, the amount of light transmitted is less, because of light absorption by the drug particles, whereas in pure nanoparticles, the amount of light transmitted is high, because of absence of the drug particles.

Table 1: Drug Release Study:

3.5 DRUG RELEASE: The release occurs by diffusion, where the drug is uniformly distributed. The invitro release of the drug by artificial biological membranes was studied. Drug release from known amounts of RIF's loaded FGPS nanoparticles was evaluated. The in-vitro drug release of RIF- loaded FGPS was studied for 75 hours at pH 7.4 by using a dialysis membrane. In the first 14 hrs, 42% of RIF was released from the nanoparticles which increased to 48% in 25 hrs. The release behavior of drug from the fish gelatin matrix when studied was found that the release may have occurred through the matrix of the nanoparticles.

S.no	Time (h)	Drug Released
1	0	0
2	1	10
3	2	18
4	4	30
5	8	45
6	14	55
7	25	68
8	47	75
9	75	82



3.6 ANTIBACTERIAL ACTIVITY STUDIES:

The antimicrobial activity of the nanoparticles was compared with that of the free drug RIF by disc diffusion method. NPs better penetrate the bacterial cell and enables better delivery of RIF to the active site, hence RIF loaded FG NPs possess high antibacterial activity against the *Mycobacterium Tuberculosis*. The antibacterial activity of drug loaded NPs were greater than that of free drug. Nano encapsulation

did not increase the antibacterial activity of RIF. Growth inhibition was compared with drug.

CONCLUSION:

A novel approach was followed for the preparation of RIF loaded FG NPs. These nanoparticles possess various therapeutic and biomedical applications. Fish gelatin was extracted successfully from the skin and fin of cat fish by acidic methods.

The fish gelatin nanoparticles were successfully extracted by a two-step

desolvation method, encapsulation and characterization. In vitro release and antibacterial activity of the FGNPs were found out to determine the efficiency of the system. Rifampicin is a bactericidal antibiotic with a wide spectrum of activity and is used to treat Mycobacterium including tuberculosis and leprosy.

It is less active against gram-negative bacteria. RIF inhibits DNA dependent RNA polymerase in bacterial cells by binding to its B subunit. The results demonstrated that the RIF loaded NPs were more effective against gram positive bacteria. The advantage of using gelatin nanoparticles as drug vehicle is that they enable controlled release of drugs.

The dosage of drug required is reduced with gelatin nanoparticles,

when compared with that through the oral route; hence side effects are significantly reduced.

ACKNOWLEDGEMENT:

I thank the Lord Almighty for his immense grace and love all through my life and during the project work. At the outset, I would like to express my sincere gratitude I express my wholehearted gratitude to Dr. S. Prakash Ph.D., Head of the Department of Biotechnology who has been guiding force and constant source of inspiration to us my sincere thanks to general manager of Indian Rare Earths Ltd, Government of India. For his constant support and guidance. I hereby express my deep sense of gratitude to all my staffs.

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